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Interactions between silver nanoparticles/silver ions and liposomes: evaluation of the potential passive diffusion of silver and effects of speciation

CAMILLE GUILLEUX, PETER G.C. CAMPBELL and CLAUDE FORTIN*

Institut national de la Recherche scientifique, INRS Eau Terre et Environnement
490 rue de la Couronne
Québec, Canada G1K 9A9

*Corresponding author
Email claude.fortin@ete.inrs.ca; Telephone (418) 654-3770

26 **Abstract**

27 Silver nanoparticles, used mainly for their antibacterial properties, are among the most common
28 manufactured nanomaterials. How they interact with aquatic organisms, especially how they cross
29 biological membranes, remains uncertain. Free Ag^+ ions, released from these nanoparticles, are
30 known to play an important role in their overall bioavailability. In this project, we have studied
31 the uptake of dissolved and nanoparticulate silver by liposomes. These unilamellar vesicles,
32 composed of phospholipids, have long been used as models for natural biological membranes,
33 notably to study the potential uptake of solutes by passive diffusion through the phospholipid
34 bilayer. The liposomes were synthesized using extrusion techniques and were exposed over time
35 to dissolved silver under different conditions where Ag^+ , AgS_2O_3^- or AgCl^0 were the dominant
36 species. Similar experiments were conducted with the complexes HgCl_2^0 and $\text{Cd}(\text{DDC})_2^0$, both of
37 which are hydrophobic and known to diffuse passively through biological membranes. The
38 uptake kinetics of Ag^+ , HgCl_2^0 and $\text{Cd}(\text{DDC})_2^0$ show no increase in internalized concentrations
39 over time, unlike AgS_2O_3^- and AgCl^0 , which appear to pass through the phospholipid bilayer.
40 These results are in contradiction with our initial hypothesis that lipophilic Hg and Cd complexes
41 would be able to cross the membrane whereas silver would not. Encapsulated tritiated water
42 inside the liposomes was shown to rapidly diffuse through the lipid bilayer, suggesting a high
43 permeability. We hypothesize that monovalent anions or complexes as well as small neutral
44 complexes with a strong negative dipole can diffuse through our model membrane. Finally,
45 liposomes were exposed to 5-nm polyvinylpyrrolidone-coated silver nanoparticles over time. No
46 significant uptake of nanoparticulate silver was observed. Neither disruption of the membrane nor
47 invagination of nanoparticles into the liposomes was observed. This suggests that the main risk
48 caused by AgNPs for non-endocytotic biological cells would be the elevation of the free silver
49 concentration near the membrane surface due to adsorption of AgNPs and subsequent
50 oxidation/dissolution.

51 Keywords: model membrane, liposome, metals, speciation, silver nanoparticles, passive diffusion.

52

53

54 **Introduction**

55 The free metal ion is normally the most chemically reactive form for many cationic trace metals
56 in the environment and it is recognized as the best predictor of their uptake and toxicity
57 (Campbell 1995). This relation between the free metal ion activity and metal uptake reflects the
58 dominant mode of transmembrane transport for cationic trace metals, namely facilitated transport
59 involving membrane-bound transporters or channels (Campbell 1995). However, one should also
60 take a close look at small and hydrophobic complexes of trace metals that are present in natural
61 waters, as they may bypass the normal membrane transport systems and enter biological cells by
62 simple passive diffusion across the lipid bilayer (Phinney and Bruland 1994). Turner and Mawji
63 (2004) reviewed the literature in this area and summarized the experimentally determined
64 octanol-water partition coefficients (K_{ow}) for neutral Al, Cu, Mn and Pb complexes (from 0.0003
65 for Al-citrate to 10,000 for Pb-diethyl-dithiocarbamate ($Pb(DDC)_2^0$)). They compared the
66 coefficients they determined for five natural waters with the literature and concluded that such
67 hydrophobic complexes are present in natural surface waters.

68 The involvement of neutral complexes in transmembrane transport is somewhat controversial,
69 notably for $AgCl^0$. Reinfelder and Chang (1999) suggested that the $AgCl^0$ complex could pass
70 through the cell membrane of the euryhaline marine microalga *Thalassiosira weissflogii* by
71 passive diffusion. They experimentally determined the octanol-water partition coefficients (K_{ow})
72 at increasing chloride concentrations to estimate the contribution of each silver chloride complex
73 and showed that $AgCl^0$ had the highest value ($K_{ow} = 0.09$), suggesting that $AgCl^0$ could diffuse
74 through the algae phospholipid bilayer more easily than other silver species. This K_{ow} , however,
75 is much lower than that of $HgCl_2^0$ (3.3, Mason et al. (1996)) and of $Cd(DDC)_2^0$ (270 ± 28 ,
76 Boullemant et al. (2009)), the internalisation of which have been shown to occur via passive
77 diffusion. In contrast, Fortin and Campbell (2000) studied silver uptake by the freshwater green
78 alga *Chlamydomonas reinhardtii* and argued against the $AgCl^0$ passive diffusion hypothesis. For
79 example, they found that silver uptake was only slightly affected when the total silver
80 concentration was fixed and the relative importance of the $AgCl^0$ complex was varied by
81 adjusting the chloride concentration.

82 Silver nanoparticles are being increasingly used and contribute to the overall mobility of silver in
83 the environment. Blaser et al. (2008) and Gottschalk et al. (2009) estimated, using theoretical
84 models based on projected use of silver nanoparticles, that nanosilver concentrations could reach
85 40-320 ng/L in European rivers and 0.09-0.43 ng/L in American surface waters. Although silver
86 nanoparticles will likely dissolve or react with suspended particles (Blaser et al. 2008), they could

87 also come into contact with aquatic organisms. However, the assimilation mechanisms of
88 nanoparticles are not well known yet (Treuel et al. 2013). Additionally, their transformations and
89 the speciation of the resulting species will directly affect their bioavailability and toxicity towards
90 aquatic organisms (Levard et al. 2012). To our knowledge, there is only one report of intact
91 nanoparticle assimilation by a unicellular organism (Miao et al. 2010). In this paper, the authors
92 suggested that silver nanoparticles were taken up by phagocytosis, but passive uptake of silver
93 nanoparticles through cell membranes could also contribute to the overall internalization.

94 Phospholipid membranes and especially liposomes, as presented in Figure 1a, have often been
95 used as abiotic models of biological membranes, especially for pharmacological research. Indeed,
96 many of the properties of these vesicles, such as osmotic swelling and permeability to small
97 solutes, are similar to those of natural membranes (Sessa and Weissmann 1968). Rusciano et al.
98 (2009) examined, for example, the interaction between nano-sized organic carbon particles and
99 liposomes. Moghadam et al. (2012) used liposomes to study the influence of the concentration
100 and coating of gold and titanium dioxide nanoparticles on membrane disruption.. The aims of the
101 present study were to determine if liposomes can be used as a model to study the passive
102 diffusion of Ag(I) and the interactions between 5-nm PVP-coated AgNPs and the lipid bilayer.
103 Large unilamellar vesicles made of egg phosphatidylcholine (PC) were prepared. PC is one of the
104 main phospholipids in natural membranes, especially in aquatic invertebrates and algae. One of
105 the objectives of this approach was to explore whether or not silver nanoparticles can cross the
106 cell membrane of small unicellular organisms such as algae. The PC gel-liquid crystalline
107 transition temperature (-2.5°C) is low enough to allow us to work at ambient temperature
108 (Koynova and Caffrey 1998). The simplicity of the membrane composition was important so that
109 only passive diffusion through the lipid bilayer could be considered. Similar experiments were
110 performed with HgCl_2^0 and $\text{Cd}(\text{DDC})_2^0$, known to be sufficiently hydrophobic to pass through the
111 biological membranes as mentioned previously, and tritiated water to evaluate the suitability or
112 the potential limits of our model membrane.

113 **Materials and methods**

114 **Buffer preparation**

115 All plasticware was soaked for 24 h in 10% HNO_3 (v/v), rinsed three times with deionized water
116 and three times with ultrapure water ($\geq 18 \text{ M}\Omega \text{ cm}$) prior to use. Phenol red and sodium
117 thiosulfate pentahydrate were obtained from Fisher Scientific. The 2-(N-morpholino)-
118 ethanesulfonic acid (MES) and 2-(N-morpholino-propanesulfonic acid (MOPS) were obtained

119 from Sigma-Aldrich. Table 1 shows the composition of the different buffer solutions used in this
120 study. The buffers were prepared by using stock solutions (0.1 M) of each of the components,
121 which had been previously filtered through 0.2 μm polycarbonate filter membranes. The pH of
122 the buffer solutions was adjusted using a 1 M NaOH solution and the ionic strength was fixed at
123 25 meq/L by addition of KNO_3 ; the pH was chosen to be environmentally relevant, based on the
124 average pH of freshwater (6.3-8.3, MDDELCC (2016)) and internal cell medium (5.5-7.5,
125 Carrozzino and Khaledi (2005)). In order to maintain the concentration gradient between the
126 exposure solution and the internal solution trapped in the liposomes, a strong ligand was added to
127 the liposomes' inner solution. We chose thiosulfate because it forms very stable hydrophilic
128 complexes with silver (AgS_2O_3^- , $\text{Ag}(\text{S}_2\text{O}_3)_2^{3-}$: $\log K_1 = 8.82$, $\log \beta_2 = 13.50$, Martell et al. (2004))
129 and mercury ($\text{Hg}(\text{S}_2\text{O}_3)_2^{2-}$, $\text{Hg}(\text{S}_2\text{O}_3)_3^{4-}$: $\log K_1 = 29.27$, $\log K_2 = 30.8$, Nyman and Salazar
130 (1961)). For cadmium, ethylenediaminetetraacetic acid (EDTA) was chosen as the internal ligand
131 ($\text{Cd}(\text{EDTA})^{2+}$, $\log K = 18.1$, Martell et al. (2004)). The ionic strength and species distribution in
132 each solution were calculated using MINEQL+ chemical equilibrium software (v.4.6; Schecher
133 and McAvoy (2001)). According to these calculations, silver and mercury were mostly (>99%)
134 bound to thiosulfate when placed in the internal buffer solution, for all tested conditions;
135 similarly, cadmium speciation in the internal buffer solution was dominated by its complex with
136 EDTA (>99%).

137 Liposomes synthesis

138 Egg yolk phosphatidylcholine (EPC) was provided by Avanti Polar Lipids. Internally threaded
139 cryogenic vials (5 mL) were obtained from Fisher Scientific. Polycarbonate filters were provided
140 by Millipore. Liposomes were prepared by the extrusion technique (Ducat et al. 2010). Egg yolk
141 phosphatidylcholine was initially dissolved in a mixture of organic solvents (9:1;
142 chloroform:methanol), kept in the freezer at -20°C . The solvents were evaporated under a gentle
143 nitrogen flow (1 h at 35°C). The cryogenic vial was then placed in a desiccator under vacuum for
144 2 h to remove traces of solvent. The lipids were then re-suspended in the internal buffer solution
145 by using a vortex mixer. Multilamellar vesicles (or MLVs) are spontaneously formed under these
146 conditions (Berger et al. 2001). Eight freeze-thaw cycles were then applied in order to break the
147 phospholipid bilayers by the formation of ice crystals formed during the freezing step (Castile and
148 Taylor 1999) and form large unilamellar vesicles. Briefly, the vial was placed in a liquid nitrogen
149 bath for 1 min, then in a water bath at 45°C for 5 min and lastly shaken on a vortex mixer for 1
150 min. The vesicles were finally passed six times through an extruding system containing two
151 stacked 200-nm polycarbonate filters (Figure S1 in the supporting information (SI)) (Ducat et al.

152 2010). Two syringes were used alternately, without changing the filter orientation, to force the
153 liposomes through the filters, minimizing losses.

154 The mean diameter and size distribution of the liposomes were analyzed by dynamic light
155 scattering (DLS) using a Malvern Zetasizer Nano-ZS instrument. Malvern folded capillary zeta
156 cells were cleaned three times with ethanol and three times with ultrapure water before use for
157 measurements. Six measures were taken at 25°C for each preparation, each measure
158 corresponding to six scans of 15 s each.

159 Size-exclusion chromatography

160 The aim of this step was to transfer the liposomes to the pH 7.4 exposure buffer solution and to
161 verify the liposomes' membrane integrity. Indeed, if there were any leakage out of the liposomes,
162 the phenol red dye, yellow in the pH 6.0 internal buffer solution, would reach the pH 7.4 outer
163 solution and turn red. Sephadex G50 Fine resin was obtained from Fisher Scientific. The 2.5 x 50
164 cm Econo-Column Chromatography columns were purchased from Bio-Rad. The transfer was
165 done by passing the liposomes through a Sephadex G50 resin filled column, used for size-
166 exclusion chromatography (SEC) and previously equilibrated with the pH 7.4 exposure buffer
167 solution. The first colored fraction (yellow), containing the liposomes, was collected and analyzed
168 on a Varian Cary 50 UV-spectrophotometer at 432 nm (Agilent Technologies). Just after the
169 fraction collection and before using the large unilamellar vesicles (LUVs), the vials containing
170 the liposomes were kept on ice to avoid potential membrane damage. The mean diameter and size
171 distribution of the liposomes in the pH 7.4 exposure buffer solution were determined again as
172 mentioned above.

173 Total phosphorus analysis

174 In order to quantify the amount of liposomes used, a relationship between the absorbance of a
175 sample at 432 nm (phenol red absorbance wavelength) and its total phosphorus concentration (g
176 P/L) was determined. The total phosphorus concentration was determined by colorimetry. Briefly,
177 a sample aliquot was diluted in a 0.2 % sulfuric acid solution. After addition of 0.5 g of potassium
178 persulfate, the solution was autoclaved for 45 min between 83 and 103 kPa. A solution of 7.5 g/L
179 ammonium paramolybdate and 0.14 g/L potassium antimonyl tartrate in 8.8% H₂SO₄ was stirred
180 together with a solution of 25 g/L ascorbic acid. This mixture was added to the autoclaved
181 solution to form a blue complex with phosphate. A standard solution of KH₂PO₄ was used to
182 establish a calibration curve and a control sample initially containing 3.54 mg P/L was used to

183 verify the method accuracy. Absorbance measurements were made on a UV-spectrophotometer at
184 885 nm. The phosphorus calibration curve is given in Figure S2 (SI).

185 The total number of phosphatidylcholine molecules per chromatographic fraction, N_{PC} , could
186 then be calculated as follows:

$$187 \quad n = C \times V = \frac{N_{PC}}{N_a} \quad (1)$$

$$188 \quad \Rightarrow N_{PC} = C \times V \times N_a = \frac{x}{31} \times V \times N_a \quad (2)$$

189 where n = amount of PC (moles), C = concentration (moles PC/L), V = fraction volume (L),
190 N_a = Avogadro constant ($6.022 \cdot 10^{23}$ mole⁻¹), x = total phosphorus concentration in the fraction
191 (g P/L).

192 The total number of liposomes per chromatographic fraction is:

$$193 \quad N_{LUV} = \frac{N_{PC}}{N_{tot}} \quad (3)$$

194 The total number of phosphatidylcholine molecules per liposome, N_{tot} , depends on the
195 liposome's diameter d (nm) (Enoch and Strittmatter 1979):

$$196 \quad N_{tot} = 17.69 \times \left(\left(\frac{d}{2} \right)^2 + \left(\frac{d}{2} - 5 \right)^2 \right) \quad (4)$$

$$197 \quad \text{Then, } N_{LUV} = \frac{\frac{x}{31} \times V \times N_a}{17.69 \times \left(\left(\frac{d}{2} \right)^2 + \left(\frac{d}{2} - 5 \right)^2 \right)} \quad (5)$$

198

199 Short term accumulation experiments

200 *Liposomes exposed to dissolved silver*

201 This preliminary experiment was done to quantify any contribution of the free silver ion, released
202 from the nanoparticles, to silver uptake by the liposomes. This was also useful to quantify the
203 potential contribution of free silver ions in the AgS_2O_3^- and the AgCl^0 experiments (Table 2).

204 Radioactive $^{110\text{m}}\text{Ag}$ (as AgNO_3 in 0.1 M HNO_3 , initial specific activity = 5.15 mCi/mL, total $[\text{Ag}]$
205 = 5 mM) was supplied by the Radioisotope Centre Polatom. Short-term (100 min) experiments
206 were performed at $\text{pH } 7.40 \pm 0.02$ with an initial concentration of 30 nM $^{110\text{m}}\text{Ag}$ in the exposure

207 solution. As radioactive silver produces radiation at 657.76 keV, every analysis was done
208 between 580 and 1020 keV on a Wizard 2 automatic gamma counter (PerkinElmer), with a
209 counting time of 300 s and a maximal counting number of 100,000 events.

210 Radioactive silver was diluted in a pH 7.4 buffer solution with or without a silver-binding ligand
211 (thiosulfate or chloride), the pH was adjusted using a 1 M NaOH solution and the ionic strength
212 was fixed with KNO₃ to reach the same ionic strength as the internal buffer held within the
213 liposomes (Tables 1 and 2). The solutions were placed in three 125-mL HDPE vials. An aliquot
214 of each solution was then taken and analyzed on the gamma counter to determine the initial silver
215 exposure concentration. An aliquot of the liposomes suspension was then added to the exposure
216 solutions and the vials were placed on a Wrist Action Shaker (Burrell) for 100 min. The liposome
217 concentration was selected so that the external silver concentration did not decrease more than
218 10% during the exposure period. The thiosulfate concentration in the inner solution (1.33 mM)
219 was chosen to ensure that it was always greater than the internal silver concentration, so that a
220 free Ag⁺ concentration gradient was maintained between the exposure solution and the solution
221 held within the liposomes.

222 In the time-course experiments, an aliquot from each vial was taken every 10 min and placed in a
223 15-mL vial containing Ambersep GT 74 resin (300 mg) (Sigma-Aldrich), a weakly acidic cation
224 exchange resin with very high affinity for soft metal ions such as mercury, silver and cadmium.
225 The vials were shaken for 5 min. After allowing the resin to settle, an aliquot of the supernatant
226 was taken and analyzed on the gamma counter (see Figure S3 in the supporting information for a
227 detailed illustration of the experimental design of these uptake experiments).

228 Similar experiments were conducted with liposomes prepared with an internal buffer solution
229 without thiosulfate (internal buffer solution (w/o trap) in Table 1) and the results were compared
230 to the previous ones. As only adsorption to the liposomes could occur in these experiments, it
231 allowed us to differentiate between uptake (C, D or E in Figure 1c) and adsorption (B in Figure
232 1c) by comparing the first two experiments: if the results are the same, only adsorption is
233 occurring. On the other hand, if there is a difference, one could conclude that silver can pass
234 through the liposome membrane.

235 *Liposomes exposed to HgCl₂⁰*

236 Similar experiments were conducted in a medium where HgCl₂⁰ was the dominant species
237 (exposure solution 4 in Table 2). Mercury was diluted in a pH 7.4 buffer solution with chloride as

238 the mercury ligand. The liposomes were exposed as explained previously for silver. Ambersep
239 GT 74 resin (500 mg) was then added to stop the exposure and bind non-adsorbed and non-
240 internalized mercury. Mercury was analysed by inductively coupled plasma – mass spectrometry
241 (ICP-MS, Model XSeries 2, Thermo Scientific). Briefly, samples were diluted in 10% HCl and
242 3% H₂O₂. Gold was also added to a concentration of 10 ppm to prevent any adsorption of Hg on
243 tube walls. Instrument response was calibrated within the expected range (0 to 28 nM) with
244 standard solutions obtained from PlasmaCAL SCP Science. An internal standard solution of ¹⁰³Rh
245 (58 nM) was used to correct analytical signal suppression (or enhancement) due to matrix effects
246 or signal fluctuations. Custom ICP Standards (SCP Science) were used as controls to verify the
247 precision and accuracy of the method (see Figure S3).

248 The mean diameter and size distribution of the liposomes exposed to mercury for 100 min were
249 analyzed once by dynamic light scattering (DLS) using a Malvern Zetasizer Nano-ZS instrument
250 to verify there was no change.

251 *Liposomes exposed to Cd(DDC)₂⁰*

252 Radioactive Cd (as CdCl₂ in 0.5 M HCl, initial specific activity = 37.1 μCi/mL, total [Cd] = 1.0
253 μM) was supplied by Eckert & Ziegler). Similar experiments were conducted in a medium where
254 Cd(DDC)₂⁰ was the dominant species (exposure solution 5 in Table 2). Cadmium was diluted in a
255 pH 7.4 buffer solution with sodium diethyl-dithiocarbamate (DDC) as the cadmium ligand. The
256 liposomes were exposed as explained before. As radioactive cadmium produces radiation at 22
257 keV, each analysis was done between 16 and 32 keV on a Wizard 2 automatic gamma counter
258 (PerkinElmer)), with a counting time of 600 s and a maximal counting number of 10,000,000
259 events (see Figure S3).

260 *Liposomes exposed to tritiated water*

261 The basic permeability of the phospholipid bilayer was determined by measuring the diffusion of
262 tritiated water from the internal to the external buffer. Tritiated water (initial specific activity = 10
263 mCi/mL) was supplied by DuPont. The liposomes were prepared in a buffer containing tritiated
264 water so as to encapsulate ³H₂O inside the vesicles. The liposomes were then transferred to the
265 pH 7.4 exposure buffer solution using the Sephadex column as described above. Fractions from
266 the column were collected every 10 or 20 mL and analysed on the liquid scintillation analyzer and
267 UV-visible spectrophotometer to quantify ³H and P respectively. Each analysis was done between

268 0 and 18.6 keV using Ecolite scintillation cocktail (MP Biomedicals) on a Tri-Carb 2910TR
269 liquid scintillation analyzer (PerkinElmer), with a counting time of 1 min.

270 *Liposomes exposed to silver nanoparticles*

271 A solution of 5-nm PVP-coated silver nanoparticles with an initial concentration of 9 mM
272 (Nanocomposix, San Diego, CA) was used in these experiments. In order to be able to compare
273 the results for silver nanoparticles with those for dissolved silver, the concentration of free silver
274 in the exposure solution 6 should be equal to that in the exposure solution 1 (Table 2).
275 Ultracentrifugation was used to determine the free silver content in AgNPs solutions of different
276 concentrations, between 42 and 463 nM, prepared from the 9 mM solution. Silver nanoparticles
277 were diluted in a solution at pH 7.4 as shown in Table 2. Ultracentrifugation tubes (Amicon
278 Ultra-15, Millipore), equipped with filters with a molecular weight cut-off (MWCO) of 3 kDa,
279 were pre-rinsed with the external buffer solution in order to remove glycerin present on the
280 membranes. Filters were then pre-equilibrated with the AgNPs solutions by successive
281 centrifugations at 3700 x g for 20 min, as dissolved silver adsorbs on the membrane surface to a
282 non-negligible extent. After each centrifugation, total and ultrafiltered Ag concentrations were
283 analyzed by ICP-MS (2% HNO₃). For example, the dissolved silver concentrations after one and
284 two centrifugations were statistically different. For the targeted 4 µg/L solution, dissolved silver
285 concentrations decreased from 1.8 to 1.4 µg/L due to adsorption on the membrane (Figure S6).
286 The equilibrium was estimated to be achieved after five successive centrifugations. The selected
287 AgNPs concentration was that for which the dissolved Ag concentration at equilibrium was about
288 20 nM. Ultracentrifugation was also used as presented above during the accumulation
289 experiments in order to monitor the potential AgNPs oxidation/dissolution through time.

290 Exposure of the liposomes to silver nanoparticles was performed in a similar way to that
291 described for dissolved metals. Exposure solution 6 (Table 2) was prepared from the 9 mM
292 AgNPs solution. The liposomes, synthesized in the internal buffer solution (containing
293 thiosulfate), were exposed for 100 min. Every 10 min, a 5 min treatment with the Ambersep GT
294 74 resin (500 mg) was applied to liposomes exposed to nanoparticles. Analyses were performed
295 by ICP-MS as explained above.

296

297 Replication and Statistics

298 Every experiment was conducted at least twice ($n \geq 2$). Data were analysed for normality using
299 the Shapiro-Wilk test and for homogeneity of variance across treatments using Levene's test.
300 Student's t-tests were run to compare distributions with a size $n = 2$. One way ANOVA test was
301 applied to compare distributions with size $n > 2$. The effect of exposure time on the accumulation
302 of metals was evaluated using linear regressions. Non-linear regression (exponential rise to
303 maximum, Boulemant et al. (2009)) was used when it best fitted the data. Statistical analyses
304 were conducted at a 95% confidence interval ($\alpha = 0.05$) and graphs were created using SigmaPlot
305 12.5.

306

307 **Results**

308 Liposomes: mean diameter and size distribution

309 The Malvern Zetasizer Nano-ZS, used to determine the mean diameter and size distribution of the
310 liposomes, is an instrument based on dynamic light scattering (DLS). The size distribution most
311 frequently found in the literature is an intensity distribution (Z-average), calculated from the
312 instrument signal intensity. However, this distribution is highly affected by the presence of big
313 particles and is reliable only for monomodal samples with a polydispersity index (PDI) < 0.1 . It
314 can be converted to a volume distribution (volume mean), which takes the particles' volume into
315 account (Malvern 2004).

316 The mean diameter and size distribution of the liposomes were determined immediately after their
317 synthesis, after their transfer to the pH 7.4 exposure solution, and once at the end of their
318 exposure to mercury (Table 3). The intensity and volume distributions were significantly different
319 after synthesis ($p < 0.05$); since the polydispersity index was higher than 0.1, the volume mean
320 was chosen as the reference value. The volume distributions after synthesis and after transfer to
321 the pH 7.4 buffer solution were also significantly different ($p < 0.05$). The size of the liposomes
322 tended to decrease after their transfer to the pH 7.4 buffer solution, from 173.0 ± 2.0 to $152.0 \pm$
323 6.0 nm in diameter. The reason for this decrease is unclear, given that the calculated ionic
324 strengths of the inner and outer solutions were similar at both pH values

325 Transfer to the pH 7.4 buffer solution

326 The liposomes (yellow fraction) eluted after 70 mL (Figure 2). The second fraction, in red, eluted
327 much later than the liposomes (elution volume = 265 mL). The background noise in absorbance at
328 432 nm was relatively low (around 0.06) and the results were reproducible: the elution volume of
329 the LUVs fraction (maximum absorbance between 70 and 75 mL) as well as the difference in
330 elution volume between fractions (around 150 mL) were similar for the three replicates.

331 Short term accumulation experiments

332 *Liposomes exposed to dissolved metals*

333 The accumulation of Ag^+ by liposomes (Figure 3a) had reached a plateau from the experiment
334 start (10 min) and no significant effect of time ($p > 0.05$) was observed on the accumulation of
335 Ag. Similar results were obtained for HgCl_2^0 (Figure 3b) and $\text{Cd}(\text{DDC})_2^0$ (Figure 3f) ($p > 0.05$).
336 On the other hand, the accumulation of AgS_2O_3^- as a function of time (Figure 3c) fitted a non-
337 linear regression as described by eq 6:

$$338 \quad f = a(1 - e^{-bt}) \quad (6)$$

$$339 \quad [\text{Ag}]_L = [\text{AgS}_2\text{O}_3^-]^0 \cdot \frac{k_i}{k_e \cdot f_L} \cdot (1 - e^{-k_e \cdot f_L \cdot t}) \quad (7)$$

340 where $[\text{Ag}]_L$ is the total Ag concentration in the liposomes ($\mu\text{mol Ag/g P}$), $[\text{AgS}_2\text{O}_3^-]^0$ the
341 concentration of the complex in the exposure solution ($\mu\text{mol/L}$), k_i the uptake constant (L/g
342 $\text{P} \cdot \text{min}$), k_e the elimination constant (min^{-1}) and f_L the labile intracellular metal fraction (eq 7,
343 derived from Boullemant et al. (2009)).

344 A significant coefficient of determination ($R^2=0.98$, $p < 0.0001$, $n=10$) was obtained, indicating a
345 strong effect of time on the accumulation of silver complexed with thiosulfate (Figure 3c). A
346 similar result was obtained for AgCl^0 (Figure 3e) ($R^2=0.90$, $p < 0.0001$, $n=10$). No statistically
347 significant accumulation was observed for the experiment without thiosulfate in the internal
348 buffer solution (Figure 3d). In the absence of a trap in the internal buffer solution, silver can
349 adsorb to the surface of the liposomes but does not accumulate inside.

350 *Liposomes exposed to tritiated water*

351 Another experiment designed to test the liposomes' permeability was performed with tritiated
352 water. It was encapsulated inside the liposomes and passed through the steric exclusion
353 chromatography column. Figure 4 presents the radiometric results associated with the collected
354 fractions. The liposomes emerged after around 70 mL, as shown previously and a radioactivity of

355 only 6 cpm/mL, linked to the tritiated water concentration, was detected in the liposomes' main
356 fraction (70-80 mL).

357 *Liposomes exposed to silver nanoparticles*

358 We compared the ultrafiltered Ag concentrations (from 9 to 40 nM) after five successive
359 centrifugations of AgNPs solutions at different concentrations. We were then able to conclude
360 that the solution at 42 nM Ag_{total} was closest to the experimental conditions with dissolved silver
361 (20 nM Ag_{dissolved}, Figure S6, SI).

362 The oxidation of AgNPs as a function of time is presented in Figure 5. At time 0, only ~40% of
363 silver was in dissolved form. After about 20 min, a decrease in total Ag concentration was
364 observed in the solution (about 60%), presumably due to Ag adsorption. Silver was then present
365 mostly as dissolved (93%) and showed little variation over time, although a small statistically
366 significant increase was observed (one way ANOVA $p < 0.05$).

367 The liposome exposure experiment to nanosilver was repeated three times under the same
368 experimental conditions. The results were gathered in Figure 6. No statistically significant
369 increase (based on linear or non-linear regression analyses) was observed. Note that in the case
370 where the raw data (and not the averages) were collected on the same graph, the increase was
371 slightly significant ($p = 0.0224$) (Figure S7, SI).

372

373 **Discussion**

374 The biotic ligand model (BLM) is used to predict the bioavailability (and potential toxicity) of
375 metals in the aquatic environment towards aquatic organisms (Campbell et al. 2002). The BLM
376 predicts that, once a metal encounters the surface of a living cell, it may bind to surface sites
377 before being transported across the membrane. Typically, adsorption occurs very rapidly whereas
378 metal accumulation increases slowly over time (Campbell et al. 2002). In the context of our
379 study, if only metal adsorption on liposomes occurs, equilibrium should be reached rapidly. This
380 is the case for Ag⁺ (cf. Figure 3a), which leads us to conclude that ionic silver did not diffuse
381 passively through the membrane of the liposomes but was only adsorbed at their surface.

382 Our results also suggest that HgCl₂⁰ (Figure 3b) and Cd(DDC)₂⁰ (Figure 3f) were also simply
383 adsorbed on the membrane of the liposomes, contrary to expectations. As mentioned in the
384 introduction, these two species are believed to be sufficiently hydrophobic ($K_{ow} = 3.3$, Mason et

385 al. (1996) and 270 ± 28 at pH 7, Boulelman et al. (2009), respectively) to pass through the lipid
386 membrane. Indeed, Mason et al. (1996) demonstrated that the coastal diatom *Thalassiosira*
387 *weissflogii* took up HgCl_2^0 by passive diffusion. Moreover, Bienvenue et al. (1984) and
388 Gutknecht (1981) studied the permeability of planar lipid bilayer membranes (PLMs), exposed to
389 the dichloromercury complex and demonstrated that it could cross the PLM by passive diffusion.
390 Finally, Boulelman et al. (2009) as well as Phinney and Bruland (1994) observed passive
391 diffusion of $\text{Cd}(\text{DDC})_2^0$ through the cell membrane of three freshwater algae and a coastal
392 diatom, respectively.

393 Based on the solubility-diffusion model, the membrane should be permeant to water and small
394 neutral solutes (Finkelstein and Cass 1968), such as glycerol and urea (Paula et al. 1996), HgCl_2^0
395 or $\text{Cd}(\text{DDC})_2^0$ (Finkelstein and Cass 1968). It is thus surprising that our model membrane does
396 not allow these species to pass. Several factors could have influenced these results. For example,
397 these species have relatively high molecular weights (272 g/mol for HgCl_2^0 and 408 g/mol for
398 $\text{Cd}(\text{DDC})_2^0$). Cohen and Bangham (1972) showed that the diffusion of non-electrolytes (estimated
399 as the ratio of the measured permeability values to the oil/water partition coefficient) into
400 liposomes tended to decrease when the molecular weight increased. Note also that the water
401 permeability values for planar lipid membranes (PLMs) are on average one order of magnitude
402 higher than those for LUVs, suggesting that LUVs may be less permeable than PLMs (Deamer
403 and Bramhall 1986). For example, the water permeability coefficient for egg PC liposomes is 2.0
404 $\mu\text{m/s}$ (Carruthers and Melchior 1983) against 40.2 $\mu\text{m/s}$ for egg PC planar lipid bilayers
405 (Finkelstein and Cass 1967). Furthermore, Shimanouchi et al. (2011) noticed that the hydration of
406 the lipid bilayer depends on its curvature. In addition, metal interactions with membranes have
407 been shown to cause dehydration of liposomes, but only at mM concentrations (Kerek and
408 Prenner (2016), Klasczyk et al. (2010), Maity et al. (2016)). This parameter, regulating the
409 phospholipid headgroup mobility, varies as a function of liposome diameter and could then be
410 one of the determining factors influencing membrane permeability.

411 On the other hand, AgS_2O_3^- and AgCl^0 were shown to be slowly internalised by liposomes, with
412 an apparent steady-state reached after 60 min of exposure (Figure 3c, e). Non-linear regressions
413 using (eq 4) allowed us to extract uptake constants k_i of 52.2 ± 4.4 mL/g P·min for AgS_2O_3^- (24.2
414 nM) and 62.5 ± 19.2 mL/g P·min for AgCl^0 (24.5 nM). There is no significant difference between
415 both uptake constants (Student's t-test, $p > 0.05$), therefore the liposomes seem to be as permeable
416 to AgCl^0 as to AgS_2O_3^- . Considering the absence of any apparent passive diffusion of the
417 lipophilic complexes HgCl_2^0 and $\text{Cd}(\text{DDC})_2^0$, the uptake of AgS_2O_3^- and AgCl^0 is puzzling. Fortin

418 and Campbell (2001) suggested that AgS_2O_3^- could be transported into algal cells via
419 sulfate/thiosulfate transport systems but to our knowledge the uptake of this complex has never
420 been tested previously on artificial membranes. Some publications on lipid bilayers (Deamer and
421 Bramhall (1986), Haydon and Hladky (1972); Sessa and Weissmann (1968)) suggest that the
422 permeability of anions is significantly greater than that of cations (ex: 10^3 times higher for Cl^-
423 than for Na^+ or K^+ , Deamer and Bramhall (1986)). This could explain our results: the anionic
424 complex AgS_2O_3^- would pass through the membrane by passive diffusion, unlike the cation Ag^+ .
425 Note that this mechanism involves an exchange of anions between the inside of the liposomes and
426 the external medium in order to respect solution electroneutrality. It may also be the case for
427 AgCl_2^- , present in non-negligible proportions in the exposure solution 3 (14.5%, Table 2). With
428 regards to the small AgCl^0 complex, the residual charges are important (with large dipoles),
429 making it a very polar solute. We hypothesize that this complex can diffuse in a manner similar to
430 anions or water molecules.

431 To determine if water molecules can diffuse through the lipid bilayer of our liposomes, we
432 compared the initial and final ^3H activities after separation of the tritiated LUVs from the tritium
433 solution. The initial ^3H activity was calculated as follows. The initial concentrated solution of
434 tritiated water has an activity of 10 000 $\mu\text{Ci}/\text{mL}$. During the liposome synthesis, this solution was
435 diluted 45 times, leading to an activity of 222 $\mu\text{Ci}/\text{mL}$ or 8 222 000 Bq/mL . The internal volume
436 of a 150-nm liposome is about $1.4 \cdot 10^{-15}$ mL and the number of liposomes per mL was $3.8 \cdot 10^{12}$
437 LUVs/mL (as determined by absorbance; see supporting information). Thus, the initial ^3H activity
438 in the liposomes was estimated to be $5.5 \cdot 10^4$ Bq/mL of solution. Experimentally, only 0.25
439 Bq/mL was detected in the main liposomes fraction. The proportion of tritiated water recovered in
440 the liposomes is thus equal to 0.00005 % of the initial activity. The tritiated water, initially used
441 for liposomes synthesis, eluted after around 220 mL. Thus, the liposomes elution time (around 1
442 h, based on the elution speed) was sufficient for the encapsulated tritiated water to leave the
443 LUVs, indicating that the liposomes are very permeable to water, as first demonstrated by
444 Bangham et al. (1965). The water permeability of lipid membranes is crucial as it allows
445 biological membranes to regulate their internal volume. The membranes exhibit a wide range of
446 water permeability coefficients, depending on membrane lipid composition and structure, chain
447 length and unsaturation, and cholesterol concentration (Deamer and Bramhall 1986). The water
448 permeability of lipid bilayers is also higher for lipids in a liquid crystalline state ($T > T_{\text{transition}}$)
449 than lipids in a gel state, which is the case in this study ($T > -2.5^\circ\text{C}$) (Huster et al. 1997).

450 When AgNPs are suspended in our exposure solutions, changes were observed (Figure 5). The
451 observed trend could be due to the oxidation of AgNPs, increasing the proportion of dissolved Ag
452 and the subsequent adsorption of Ag on the container walls. Liposomes exposed to a low
453 concentration of silver nanoparticles showed no significant increase in Ag accumulation (Figure
454 6). This is consistent with the fact that no studies have shown that silver nanoparticles can pass
455 through the phospholipid membrane by passive diffusion. Le Bihan et al. (2009) studied the
456 invagination of silica nanoparticles by liposomes. They indicated that this process was very rapid
457 and that it would have been difficult to analyze it without using a method to slow it down. Thus,
458 they covered silica nanoparticles with gold nanoparticles (positively charged, 10 nm) which made
459 it possible to slow down the liposomes spreading on the silica surface. They were then able to
460 observe the intermediate steps of the engulfment process by cryo-TEM. If an invagination of
461 AgNPs-PVPs by liposomes had occurred, its observation would not have been possible under our
462 experimental conditions. It would have been possible to apply a treatment similar to that set up by
463 Le Bihan et al. (2009) in order to slow down the process and to observe or not this invagination,
464 within the 20 to 30 min where silver nanoparticles are still present and relatively intact in solution
465 (Figure 5). Nevertheless, based on Le Bihan et al. (2009), our AgNPs with a size less than or
466 equal to 5 nm would not possess sufficient adhesion strength to cause invagination and could only
467 adsorb to the surface of the liposomes. Moreover, considering the small amounts of silver found
468 associated with the liposomes (on average 38.3 $\mu\text{mol Ag} / \text{g P}$, corrected for the residual amount
469 of Ag), we can hypothesize that the invagination of silver nanoparticles is unlikely and that
470 AgNPs only adsorbed to the surface of the liposomes, as has been shown by Wang et al. (2016).

471

472 **Conclusion**

473 The objective of this study was to test if nanoparticulate silver could cross a lipid bilayer. To do
474 this we used 150-nm liposomes made of phosphatidylcholine. Because nanoparticulate silver
475 always release dissolved ions, we first had to characterize the passive diffusion of dissolved
476 species of Ag(I). This was done by performing short term experiments under different conditions
477 where Ag^+ , AgS_2O_3^- or AgCl^0 were the dominant species. The permeability of liposomes was also
478 tested with HgCl_2^0 , $\text{Cd}(\text{DDC})_2^0$ and $^3\text{H}_2\text{O}$. Our liposomes proved to be impermeable to ionic and
479 nanoparticulate silver. Considering that we used nanoparticles among the smallest available on
480 the market with the most neutral coating which would favor its passive diffusion across a lipid
481 bilayer, our results suggest that nanoparticles cannot diffuse through a bilipid membrane.

482 On the other hand, it appeared that our artificial lipid bilayer could be more permeable to anions
483 such as AgS_2O_3^- than to cations. However, this is not an inherent property of biological
484 membranes of living organisms. Although liposomes have often been used to study the
485 interaction between contaminants and biological membranes, there remains a large gap between
486 LUVs and living cells. Indeed, the hydrophobic complexes HgCl_2^0 and $\text{Cd}(\text{DDC})_2^0$ did not pass
487 through the phospholipid bilayer of our liposomes, contrary to what have been previously
488 demonstrated for biological membranes. Therefore an extrapolation of the liposomes results to
489 toxicological studies must be made with caution.

490

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495 **References**

496

497 Bangham AD, Standish MM, Watkins JC (1965) Diffusion of univalent ions across the lamellae
498 of swollen phospholipids. *J Mol Biol* 13:238-252 doi:10.1016/S0022-2836(65)80093-6

499 Berger N, Sachse A, Bender J, Schubert R, Brandl M (2001) Filter extrusion of liposomes using
500 different devices: comparison of liposome size, encapsulation efficiency, and process
501 characteristics. *Int J Pharm* 223:55-68 doi:10.1016/S0378-5173(01)00721-9

502 Bienvenue E, Boudou A, Desmazes JP, Gavach C, Georgescauld D, Sandeaux J, Sandeaux R,
503 Seta P (1984) Transport of mercury compounds across bimolecular lipid membranes:
504 effect of lipid composition, pH and chloride concentration. *Chem Biol Interact* 48:91-101
505 doi:10.1016/0009-2797(84)90009-7

506 Blaser SA, Scheringer M, MacLeod M, Hungerbuhler K (2008) Estimation of cumulative aquatic
507 exposure and risk due to silver: Contribution of nano-functionalized plastics and textiles.
508 *Sci Total Environ* 390:396-409 doi:10.1016/j.scitotenv.2007.10.010

509 Boullemant A, Lavoie M, Fortin C, Campbell PGC (2009) Uptake of Hydrophobic Metal
510 Complexes by Three Freshwater Algae: Unexpected Influence of pH. *Environ Sci
511 Technol* 43:3308-3314 doi:10.1021/es802832u

512 Campbell PGC (1995) Interactions between trace metals and aquatic organisms: a critique of the
513 free-ion activity model. In: Tessier A, Turner DR (eds) *Metal speciation and
514 bioavailability in aquatic systems*. John Wiley & Sons Ltd, pp 45-102

515 Campbell PGC, Errécalde O, Fortin C, Hiriart-Baer VP, Vigneault B (2002) Metal bioavailability
516 to phytoplankton—applicability of the biotic ligand model. *Comp Biochem Physiol C:
517 Pharmacol Toxicol* 133:189-206 doi:10.1016/S1532-0456(02)00104-7

518 Carrozzino JM, Khaledi MG (2005) pH effects on drug interactions with lipid bilayers by
519 liposome electrokinetic chromatography. *J Chromatogr A* 1079:307-316
520 doi:10.1016/j.chroma.2005.04.008

521 Carruthers A, Melchior DL (1983) Studies of the relationship between bilayer and water
522 permeability and bilayer physical state. *Biochem* 22:5797-5807 doi:10.1021/bi00294a018

523 Castile JD, Taylor KMG (1999) Factors affecting the size distribution of liposomes produced by
524 freeze-thaw extrusion. *Int J Pharm* 188:87-95 doi:10.1016/S0378-5173(99)00207-0

525 Cohen BE, Bangham AD (1972) Diffusion of small nonelectrolytes across liposomes membranes.
526 *Nature* 236:173-& doi:10.1038/236173a0

527 Deamer DW, Bramhall J (1986) Permeability of lipid bilayers to water and ionic solutes. *Chem
528 Phys Lipids* 40:167-188 doi:10.1016/0009-3084(86)90069-1

529 Ducat E, Brion M, Lecomte F, Evrard B, Piel G (2010) The experimental design as practical
530 approach to develop and optimize a formulation of peptide-loaded liposomes. AAPS
531 PharmSciTech 11:966-975 doi:10.1208/s12249-010-9463-3

532 Enoch HG, Strittmatter P (1979) Formation and properties of 1000-Å-diameter, single-bilayer
533 phospholipid vesicles. Proc Nat Acad Sci USA 76:145-149 doi:10.1073/pnas.76.1.145

534 Finkelstein A, Cass A (1967) Effect of cholesterol on the water permeability of thin lipid
535 membranes. Nature 216:717-718 doi:10.1038/216717a0

536 Finkelstein A, Cass A (1968) Permeability and electrical properties of thin lipid membranes. J
537 Gen Physiol 52:145-172 doi:10.1085/jgp.52.1.145

538 Fortin C, Campbell PGC (2000) Silver uptake by the green alga *Chlamydomonas reinhardtii* in
539 relation to chemical speciation: Influence of chloride. Environ Toxicol Chem 19:2769-
540 2778 doi:10.1002/etc.5620191123

541 Fortin C, Campbell PGC (2001) Thiosulfate enhances silver uptake by a green alga: Role of anion
542 transporters in metal uptake. Environ Sci Technol 35:2214-2218 doi:10.1021/es0017965

543 Gottschalk F, Sonderer T, Scholz RW, Nowack B (2009) Modeled environmental concentrations
544 of engineered nanomaterials (TiO₂, ZnO, Ag, CNT, fullerenes) for different regions.
545 Environ Sci Technol 43:9216-9222 doi:10.1021/es9015553

546 Gutknecht J (1981) Inorganic mercury (Hg²⁺) transport through lipid bilayer membranes. J
547 Membr Biol 61:61-66 doi:10.1007/bf01870753

548 Haydon DA, Hladky SB (1972) Ion transport across thin lipid-membranes - critical discussion of
549 mechanisms in selected systems. Q Rev Biophys 5:187-282
550 doi:10.1017/S0033583500000883

551 Huster D, Jin AJ, Arnold K, Gawrisch K (1997) Water permeability of polyunsaturated lipid
552 membranes measured by O-17 NMR. Biophys J 73:855-864 doi:10.1016/S0006-
553 3495(97)78118-9

554 Kerek EM, Prenner EJ (2016) Inorganic cadmium affects the fluidity and size of phospholipid
555 based liposomes. Biochimica et Biophysica Acta (BBA) - Biomembranes 1858:3169-
556 3181 doi:10.1016/j.bbamem.2016.10.005

557 Klasczyk B, Knecht V, Lipowsky R, Dimova R (2010) Interactions of Alkali Metal Chlorides
558 with Phosphatidylcholine Vesicles. Langmuir 26:18951-18958 doi:10.1021/la103631y

559 Koynova R, Caffrey M (1998) Phases and phase transitions of the phosphatidylcholines. Biochim
560 Biophys Acta, Biomembr 1376:91-145 doi:10.1016/s0304-4157(98)00006-9

561 Le Bihan O et al. (2009) Cryo-electron tomography of nanoparticle transmigration into liposome.
562 J Struct Biol 168:419-425 doi:10.1016/j.jsb.2009.07.006

563 Levard C, Hotze EM, Lowry GV, Brown GE, Jr. (2012) Environmental transformations of silver
564 nanoparticles: impact on stability and toxicity. *Environ Sci Technol* 46:6900-6914
565 doi:10.1021/es2037405

566 Maity P, Saha B, Kumar GS, Karmakar S (2016) Binding of monovalent alkali metal ions with
567 negatively charged phospholipid membranes. *Biochimica Et Biophysica Acta-*
568 *Biomembranes* 1858:706-714 doi:10.1016/j.bbamem.2016.01.012

569 Malvern (2004) Zetasizer nano series user manual - MAN0317 Issue 2.1. Malvern Instruments
570 Ltd.

571 Martell AE, Smith RM, Motekaitis RJ (2004) NIST critically selected stability constants of metal
572 complexes v. 8.0. National Institute of Standards and Technology, Gaithersburg, MD,
573 USA

574 Mason RP, Reinfelder JR, Morel FMM (1996) Uptake, toxicity, and trophic transfer of mercury
575 in a coastal diatom. *Environ Sci Technol* 30:1835-1845 doi:10.1021/es950373d

576 MDDELCC (2016) Suivi de la qualité des rivières et petits cours d'eau.
577 http://www.mddelcc.gouv.qc.ca/eau/eco_aqua/rivieres/annexes.htm#ph. Accessed 27
578 October 2016.

579 Miao AJ, Luo ZP, Chen CS, Chin WC, Santschi PH, Quigg A (2010) Intracellular uptake: A
580 possible mechanism for silver engineered nanoparticle toxicity to a freshwater alga
581 *Ochromonas danica*. *PLoS One* 5:e15196 doi:e1519610.1371/journal.pone.0015196

582 Moghadam BY, Hou WC, Corredor C, Westerhoff P, Posner JD (2012) Role of nanoparticle
583 surface functionality in the disruption of model cell membranes. *Langmuir* 28:16318-
584 16326 doi:10.1021/la302654s

585 Nyman CJ, Salazar T (1961) Complex ion formation of mercury(II) and thiosulfate ion. *Anal*
586 *Chem* 33:1467-1469 doi:10.1021/ac60179a005

587 Paula S, Volkov AG, VanHoek AN, Haines TH, Deamer DW (1996) Permeation of protons,
588 potassium ions, and small polar molecules through phospholipid bilayers as a function of
589 membrane thickness. *Biophys J* 70:339-348 doi:10.1016/S0006-3495(96)79575-9

590 Phinney JT, Bruland KW (1994) Uptake of lipophilic organic Cu, Cd, and Pb complexes in the
591 coastal diatom *Thalassiosira weissflogii*. *Environ Sci Technol* 28:1781-1790
592 doi:10.1021/es00060a006

593 Reinfelder JR, Chang SI (1999) Speciation and microalgal bioavailability of inorganic silver.
594 *Environ Sci Technol* 33:1860-1863 doi:10.1021/es980896w

595 Rusciano G, De Luca AC, Pesce G, Sasso A (2009) On the interaction of nano-sized organic
596 carbon particles with model lipid membranes. *Carbon* 47:2950-2957
597 doi:10.1016/j.carbon.2009.06.042

598 Schecher WD, McAvoy D (2001) MINEQL+: A Chemical Equilibrium Modeling System. 4.62
599 edn. Environmental Research Software, Hallowell, ME, USA

600 Sessa G, Weissmann G (1968) Phospholipid vesicles (liposomes) as a model for biological
601 membranes. *J Lipid Res* 9:310-318

602 Shimanouchi T, Sasaki M, Hiroiwa A, Yoshimoto N, Miyagawa K, Umakoshi H, Kuboi R (2011)
603 Relationship between the mobility of phosphocholine headgroups of liposomes and the
604 hydrophobicity at the membrane interface: A characterization with spectrophotometric
605 measurements. *Colloid Surf B-Biointerfaces* 88:221-230
606 doi:10.1016/j.colsurfb.2011.06.036

607 Treuel L, Jiang XE, Nienhaus GU (2013) New views on cellular uptake and trafficking of
608 manufactured nanoparticles. *J R Soc Interface* 10:14 doi:10.1098/rsif.2012.0939

609 Turner A, Mawji E (2004) Hydrophobicity and octanol-water partitioning of trace metals in
610 natural waters. *Environ Sci Technol* 38:3081-3091

611 Villarreal MR (2007) Cross section of a liposome via wikimedia.org (public property).

612 Wang Q, Lim M, Liu X, Wang Z, Chen KL (2016) Influence of solution chemistry and soft
613 protein corona on the interactions of silver nanoparticles with model biological
614 membranes. *Environ Sci Technol* 50:2301-2309 doi:10.1021/acs.est.5b04694

615

Table 1. Composition of the buffer solutions (ionic strength and speciation calculated using MINEQL+ v.4.6)

Buffer solutions	Composition	pH	I (mM)	Speciation
Internal buffer solution	Phenol red sodium salt 6.0 mM; MES acid buffer 5.0 mM; Na ₂ S ₂ O ₃ 1.33 mM; NaOH 2.4 mM; KNO ₃ 15.9 mM.	6.0	25.0	99.2 % Ag(S ₂ O ₃) ₂ ³⁻ 65.4 % Hg(S ₂ O ₃) ₂ ²⁻ 34.6 % Hg(S ₂ O ₃) ₃ ⁴⁻
Internal buffer solution (w/o trap)	Phenol red sodium salt 6.0 mM; MES acid buffer 5.0 mM; NaOH 2.4 mM; KNO ₃ 23.1 mM.	6.0	25.0	98.7 % Ag ⁺ 99.9% Hg ²⁺ 97% Cd ²⁺
Internal buffer solution (EDTA)	Phenol red sodium salt 6.0 mM; MES acid buffer 5.0 mM; EDTA 2.0 mM; NaOH 2.4 mM; KNO ₃ 13.3 mM.	6.0	25.0	99.9 Cd(EDTA) ²⁻
Exposure buffer solution	MOPS acid buffer 7.5 mM ; NaOH 5.6 mM ; KNO ₃ 19.9 mM	7.4	25.0	/

Table 2. Composition of the exposure solutions, after dilution with the liposome dispersion (ionic strength and speciation calculated using MINEQL+ v.4.6).

	Composition	pH	I (mM)	Speciation
Exposure solution 1	MOPS acid buffer 7.2 mM; NaOH 14.7 mM; AgNO ₃ 30 nM; KNO ₃ 15.4 mM	7.4	25.0	Ag ⁺ 99.1 %
Exposure solution 2	MOPS acid buffer 7.0 mM; NaOH 14.7 mM; AgNO ₃ 30 nM; Na ₂ S ₂ O ₃ 173.2 nM; KNO ₃ 15.5 mM	7.4	25.0	AgS ₂ O ₃ ⁻ 96.9 %; Ag(S ₂ O ₃) ₂ ³⁻ 1.2 %; Ag ⁺ 1.9 %
Exposure solution 3	MOPS acid buffer 7.0 mM; NaOH 14.8 mM; NaCl 2.5 mM; AgNO ₃ 30 nM ;KNO ₃ 12.9 mM	7.4	25.0	AgCl ⁰ 67.2 %; AgCl ₂ ⁻ 14.5 %; Ag ⁺ 18.1 %
Exposure solution 4	MOPS acid buffer 6.8 mM; NaCl 4.9 mM; NaOH 5.2 mM; HgCl ₂ 146.9 nM; KNO ₃ 15.4 mM	7.4	25.0	HgCl ₂ ⁰ 42.7 %; HgClOH ⁰ 45.4 %; HgCl ₃ ⁻ 2.1 %; Hg(OH) ₂ ⁰ 9.8 %
Exposure solution 5	MOPS acid buffer 6 mM; Na-DDC 700 nM; NaOH 4.8 mM; Cd(NO ₃) ₂ 150 nM; KNO ₃ 20.8 mM	7.4	25.0	Cd(DDC) ₂ ⁰ 99.9 %
Exposure solution 6	MOPS acid buffer 7.5 mM; NaOH 5.6 mM; AgNPs-PVP 72.5 nM; KNO ₃ 19.8 mM	7.4	25.0	Ag ⁺ 98.9 % (for dissolved silver, disregarding the presence of AgNPs)

Table 3. Size distributions of the liposomes, determined by dynamic light scattering, after their synthesis, their transfer to the pH 7.4 buffer solution and their exposure to silver. Mean \pm standard deviation.

	After synthesis (n=4) PdI* = 0.125 ± 0.02	After transfer to the pH 7.4 buffer solution (n=6) PdI* = 0.112 ± 0.005	After exposure to mercury (n=1) PdI* = 0.160
Z-average diameter	$161.8 \pm 1.6 \text{ nm}^a$	$151.2 \pm 5.6 \text{ nm}^c$	142.5 nm
Volume mean diameter	$173.0 \pm 2.0 \text{ nm}^b$	$152.0 \pm 6.0 \text{ nm}^c$	144.1 nm

*PdI : Polydispersity Index

Values with different lower case letters are significantly different ($p < 0.05$).

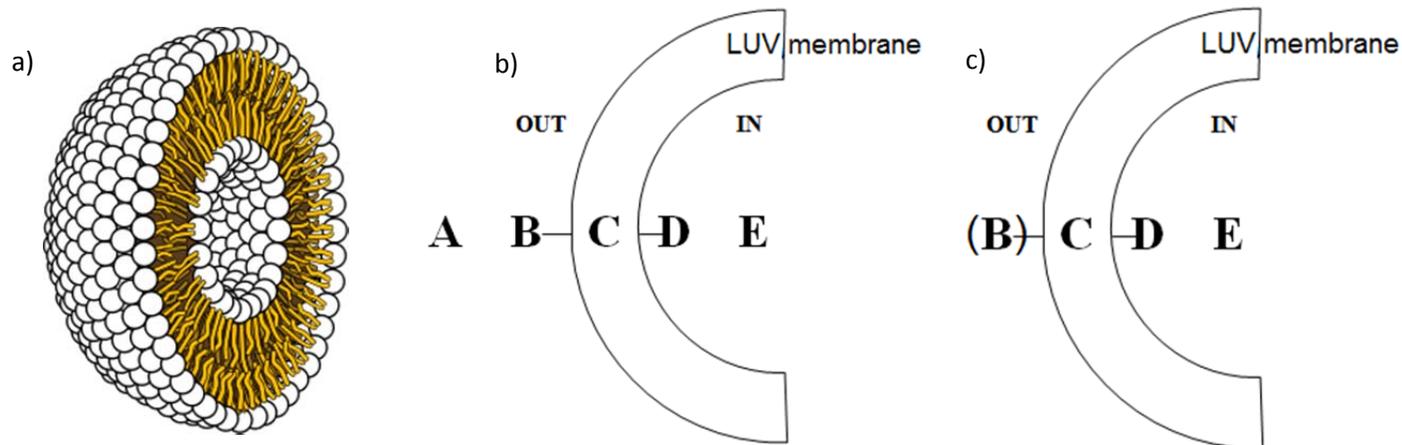


Figure 1. Cross section of a liposome (Villarreal 2007) a) and potential metal localizations after interaction with the liposomes: A. in the bulk solution, B. adsorbed at the surface of the liposomes, C. inside the lipid bilayer, D. adsorbed at the surface of the liposome in the inner solution, E. in the internal solution before b) and after c) treatment with Ambersep GT74 resin. (B) in Figure 1c) : The Ambersep GT74 resin may not be 100% efficient in removing metal adsorbed at the surface of the liposomes.

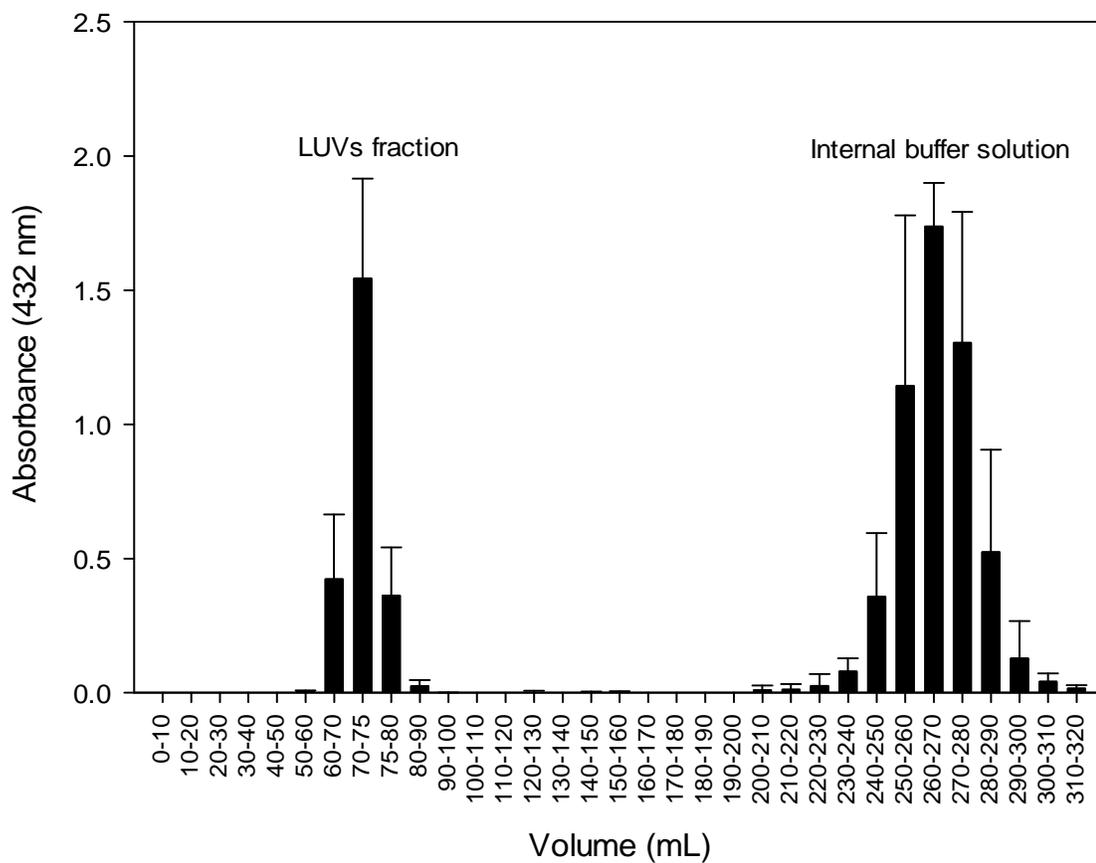


Figure 2. Presence of liposomes as determined by absorbance at 432 nm after the transfer of the liposomes to the pH 7.4 buffer solution. Liposomes were separated from the buffer solution by size exclusion chromatography. Eluant was collected in 10 mL fractions. Mean \pm standard deviation (n=3).

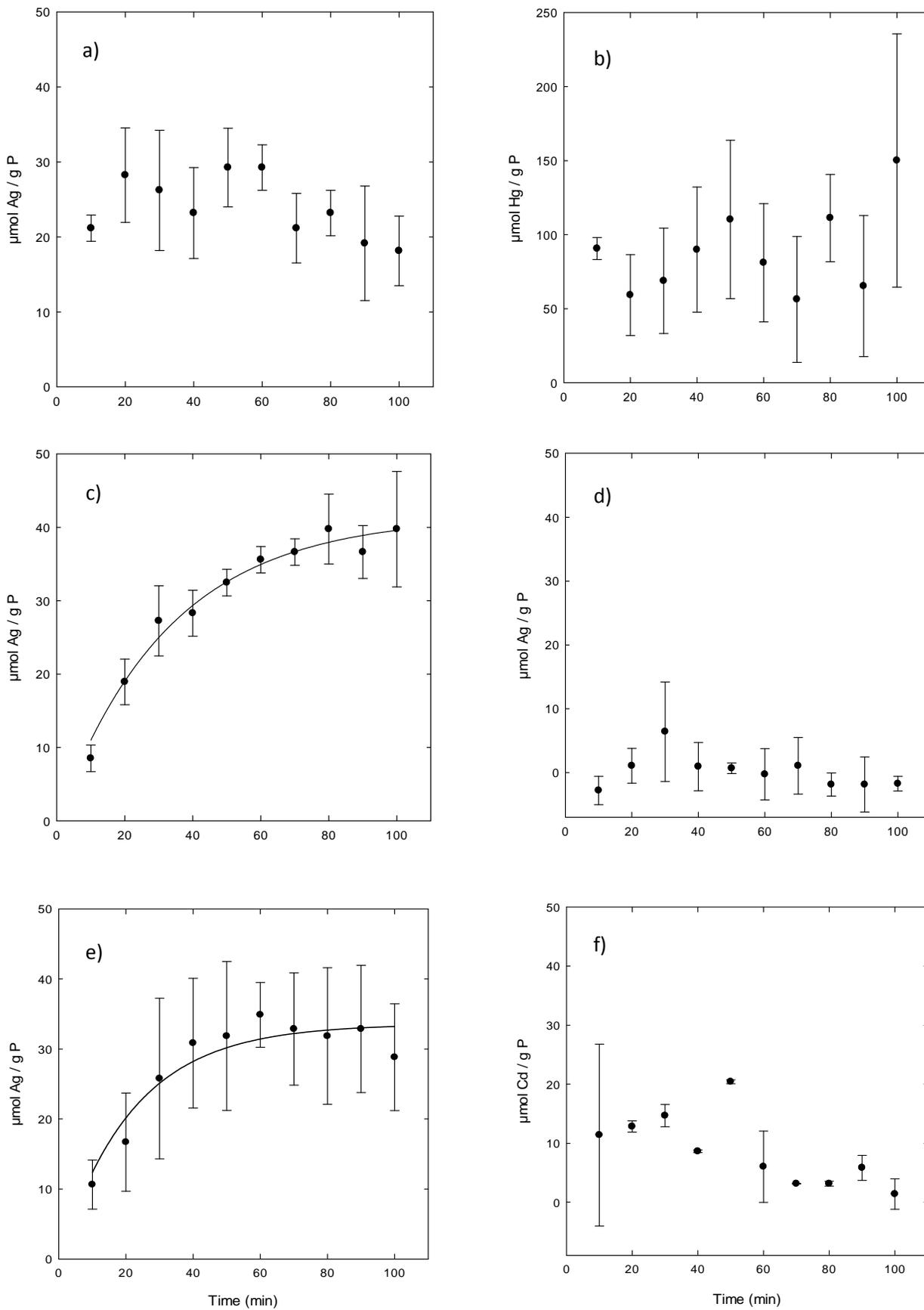


Figure 3. Accumulation of a) Ag⁺ b) HgCl₂⁰ c) AgS₂O₃⁻ d) AgS₂O₃⁻ (without internal metal trap) e) AgCl⁰ f) Cd(DDC)₂⁰ by liposomes over time, corrected for the residual quantity of dissolved metal. Mean ± standard deviation (n=3). No statistically significant increase observed for a) b) d) and f) (non-linear regression, p > 0.05).

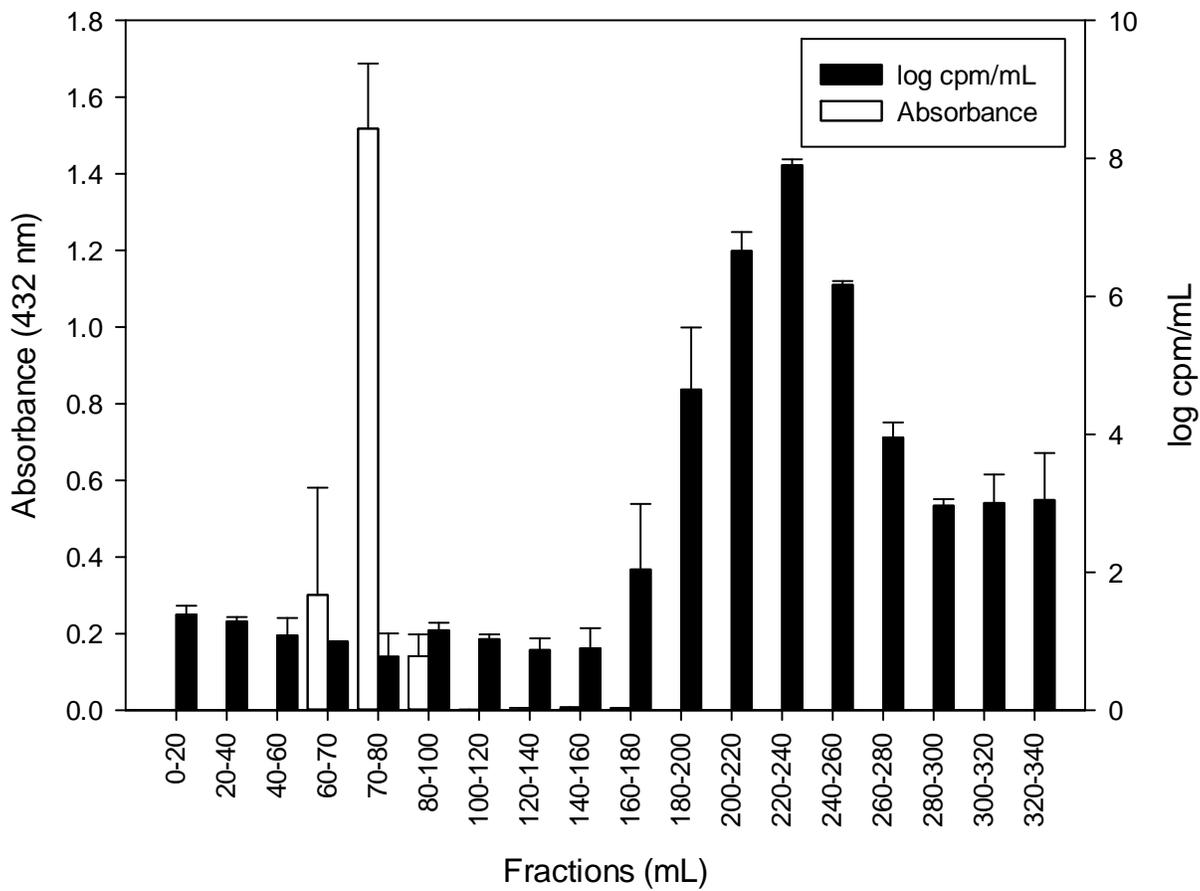


Figure 4. Presence of liposomes as determined by absorbance at 432 nm and tritium activity determined in each fraction collected from a steric exclusion column. Mean \pm standard deviation (n=2).

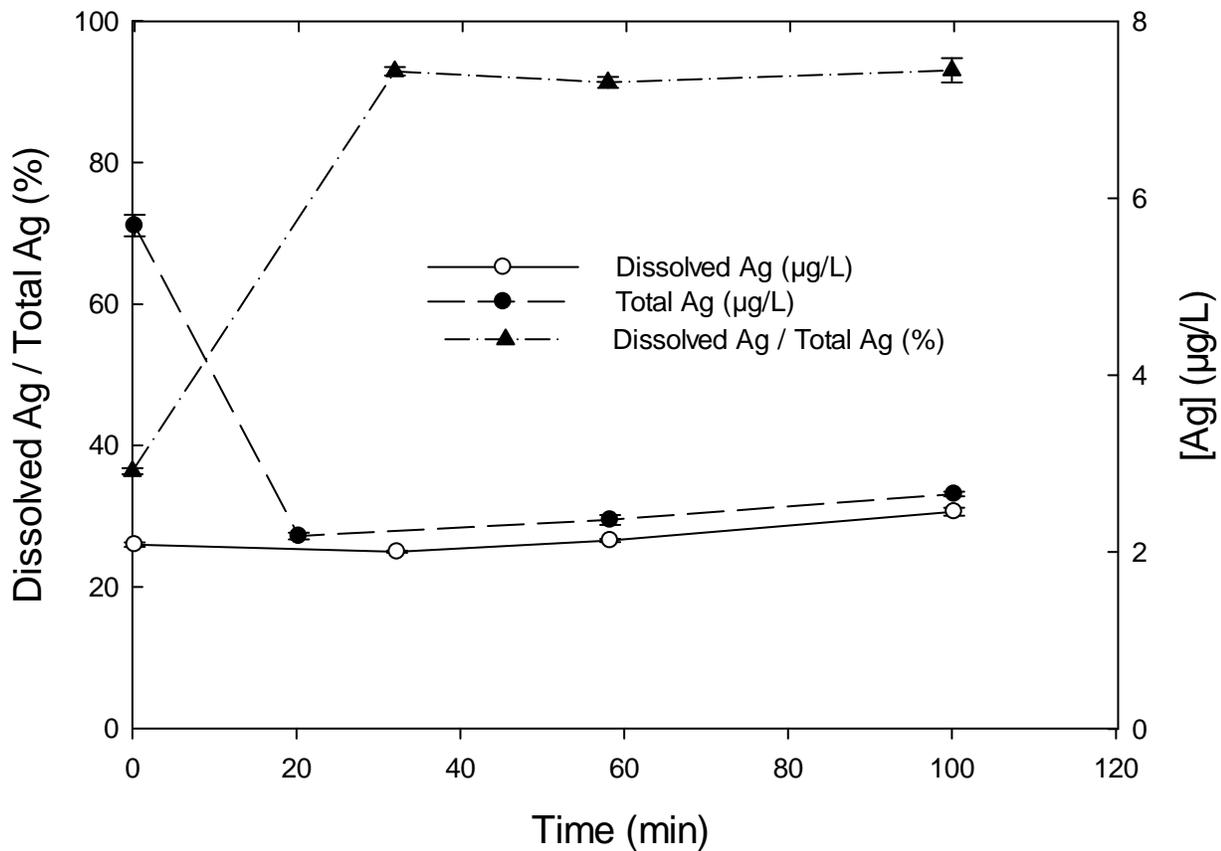


Figure 5. Oxidation of AgNPs as a function of time in exposure solution 6 (MOPS acid buffer 7.5 mM ; NaOH 5.6 mM ; AgNPs-PVP 72.5 nM ; KNO₃ 19.8 mM) and in the presence of liposomes. Mean ± standard deviation (n = 3). A small statistically significant increase observed for dissolved silver (one way ANOVA p < 0.05).

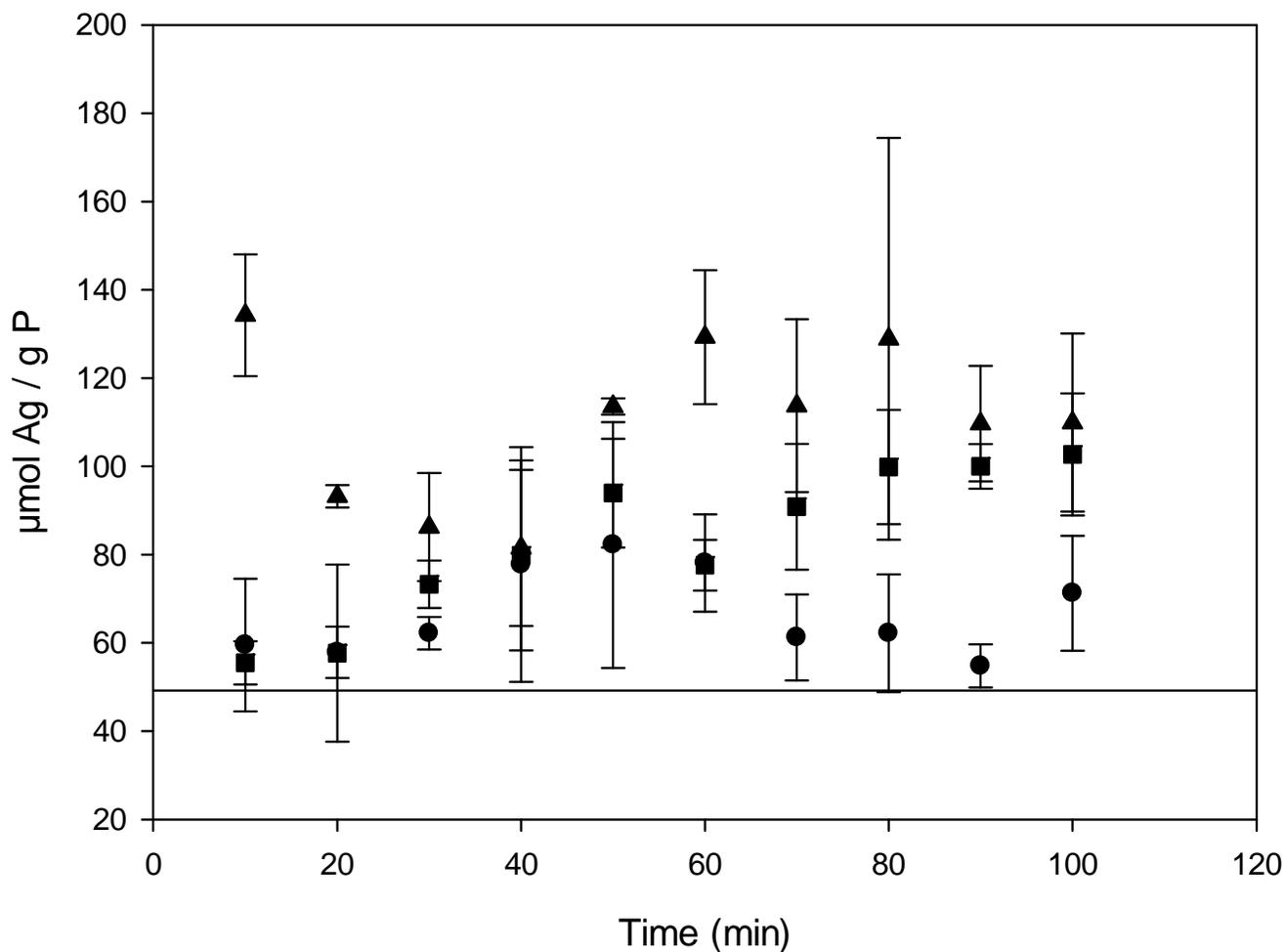


Figure 6. Accumulation of Ag by liposomes over time when exposed to AgNPs. The horizontal line corresponds to the residual quantity of dissolved metal. Mean \pm standard deviation (n=3). Each set of symbols corresponds to one experiment. No statistically significant increase observed (linear and non-linear regression : exponential rise to maximum, Boullemant et al. (2009)).